Abstract—This paper presents a classification-driven biomedical image retrieval framework based on image filtering and similarity fusion by employing supervised learning techniques. In this framework, the probabilistic outputs of a multiclass support vector machine (SVM) classifier as category prediction of query and database images are exploited at first to filter out irrelevant images, thereby reducing the search space for similarity matching. Images are classified at a global level according to their modalities based on different low-level, concept, and keypoint-based features. It is difficult to find a unique feature to compare images effectively for all types of queries. Hence, a query-specific adaptive linear combination of similarity matching approach is proposed by relying on the image classification and feedback information from users. Based on the prediction of a query image category, individual precomputed weights of different features are adjusted online. The prediction of the classifier may be inaccurate in some cases and a user might have a different semantic interpretation about retrieved images. Hence, the weights are finally determined by considering both precision and rank order information of each individual feature representation by considering top retrieved relevant images as judged by the users. As a result, the system can adapt itself to individual searches to produce query-specific results. Experiment is performed in a diverse collection of 5,000 biomedical images of different modalities, body parts, and orientations. It demonstrates the efficiency (about half computation time compared to search on entire collection) and effectiveness (about 10%–15% improvement in precision at each recall level) of the retrieval approach.

Index Terms—Classification, classifier combination, content-based image retrieval (CBIR), medical imaging, relevance feedback (RF), similarity fusion.

I. INTRODUCTION

With the advent of imaging, clinical care could be significantly impacted with improved image handling. In recent years, rapid advances of software and hardware technology have eased the problem of maintaining large medical image collections. These images constitute an important source of anatomical and functional information for the diagnosis of diseases, medical research, and education. Effectively and efficiently searching in these large image collections poses significant technical challenges as the characteristics of the medical images differ significantly from other general purpose images.

The image modality reveals anatomical and/or functional information of different body parts and pathologies. Each imaging modality presents challenges for acquisition, storage [1], and retrieval. Currently, the images are retrieved primarily using text-based searches [1], [2]. Search results in medical collections might be improved by combining text attribute-based search capability with low-level visual features computed directly on the image content, commonly known as the content-based image retrieval (CBIR) [2], [3].

During the last decade, several medical CBIR prototypes have been proposed [2], [4]–[8]. Majority of these are developed around a specific imaging modality and retrieval methods in these systems are task specific. There are a few systems that have a goal of creating CBIR systems for heterogeneous image collections [7]–[9]. To enable effective search in a large medical image collection of diverse modalities, it might be advantageous for a retrieval system to be able to recognize the image class prior to any kind of postprocessing or similarity matching [10]. A successful categorization of images would greatly enhance the performance of a CBIR system by filtering out irrelevant images and, thereby, reducing the search space. For example, to search posteroanterior (PA) chest X-rays with an enlarged heart in a radiographic collection, database images at first can be prefiltered with automatic categorization according to modality (e.g., X-ray), body part (e.g., chest), and orientation (e.g., PA) at different levels. The later similarity matching can be performed between query and images in the filtered set to find the enlarged heart as a distinct visual property. CBIR search under a specific modality and body part based on the automatic categorization of images would likely to perform better. In addition, the automatic classification of images could be utilized to adjust the feature weights in similarity matching at query time. For example, a color feature should have more weight for the images under the category of microscopic pathology or dermatology, whereas edge features are more important for the radiographs and texture-related features are important for CT or MRI images.

Some approaches have been explored in recent years to automatically classify medical image collections into multiple semantic categories for effective retrieval [10]–[12]. For example, in [11], the automatic categorization of 6231 radiological images into 81 categories is examined by utilizing a combination of low-level global texture features with low-resolution scaled images and a K-nearest-neighbor (KNN) classifier. Although these approaches demonstrate promising results for medical image classification at a global level, they do not directly relate classification to retrieval. Another effective approach for improving
category prediction (B), the predefined category-specific feature weights are utilized in a linear combination of similarity matching function as shown in the middle portion (F). After obtaining a ranked-based retrieval result (as shown in the left side of the Fig. 1), users next provide the feedback about relevant images and that information is utilized to update the final feature weights for the next retrieval iterations.

The rest of the paper is organized as follows. Section II presents the different feature representation schemes at the concepts, keypoints, and low-level feature spaces. Section III describes the image categorization and filtering approaches at a global level by utilizing the multiclass SVM. The similarity fusion approach based on image classification and RF is presented in Section IV. The experiments and the analysis of the results are presented in Sections V and VI, respectively, and finally Section VII provides the conclusion.

II. IMAGE FEATURE REPRESENTATION

The performance of a classification and/or retrieval system depends on the underlying image representation, usually in the form of a feature vector. In a heterogeneous medical image collection, it is possible to identify specific local patches in images that are perceptually and/or semantically distinguishable, such as homogeneous texture patterns in gray level radiological images, differential color, and texture structures in microscopic pathology and dermoscopic images. The variation in the local patches can be effectively modeled as local concepts [16] analogous to the keywords in text documents by using any supervised learning-based classification techniques, such as the SVM [16].

For the SVM training, the initial input to the system is the feature vector set of the patches along with their manually assigned corresponding concept labels. Images in the dataset are annotated with the concept labels by fixed partitioning each image \( I_j \) into \( l \) regions as \( \{ x_{i_1}, \ldots, x_{i_l}, \ldots, x_{i_L} \} \), where each \( x_{i_k} \in \mathbb{R}^d \) is a combined color and texture feature vector. For each \( x_{i_k} \), the concept probabilities are determined by the prediction of the multiclass SVMs as [17]

\[
    p_{i_k} = P(y = i|x_{i_k}), 1 \leq i \leq L. \tag{1}
\]

Finally, the category label of \( x_{i_k} \) is determined as \( c_m \), which is the label of the category with the maximum probability score. Based on this encoding scheme, an image \( I_j \) is represented as a vector of weighted concepts as

\[
    f_{ij}^{\text{concept}} = [w_{i_1}, \ldots, w_{i_l}, \ldots, w_{i_L}]^T \tag{2}
\]

where each \( w_{i_k} \) denotes the weight of a concept \( c_i, 1 \leq i \leq L \) in image \( I_j \), depending on its information content. The popular “tf-idf” term-weighting scheme [18] is used in this paper, where the element \( w_{i_j} \) is expressed as the product of local and global weights.

In a heterogeneous medical collection with multiple modalities, images are often captured with different views, imaging and lighting conditions, similar to the real world photographic images. Ideally, the representation of such images must be flexible enough to cope with a large variety of visually different instances under the same category or modality, yet keeping the discriminative power between images of different modalities.

In this paper, we extract such robust and invariant features from images as “bag of keypoints” [19].
In addition to the previous features, the MPEG-7 [20]-based color layout descriptor (CLD) $f^{cld}$ and edge histogram descriptor (EHD) $f^{ehd}$ and descriptors from the lucene image retrieval library [21], such as fuzzy color texture histogram (FCTH) $f^{fcth}$ and color edge direction descriptor (CEDD) $f^{cedd}$ are extracted to represent images from different perspectives.

III. MULTICLASS SVM-BASED CATEGORIZATION

The variation of the medical image categories at a global level (e.g., modalities, body parts, and orientations) can be effectively modeled by using any supervised learning techniques. The SVM [22] is used to classify images to multiple categories. A number of methods have been proposed for its extension to multiclass problems to separate $M$ mutually exclusive classes essentially by solving many two-class problems and combining their predictions in various ways [23]. In this research, we utilize a multiclass classification method by combining all pairwise comparisons of binary SVM classifiers, known as one-against-one or pairwise coupling (PWC) [17]. PWC constructs binary SVM’s between all possible pairs of classes. Hence, this method uses $M \times (M - 1)/2$ binary classifiers, each of which provides a partial decision for classifying a data point. During the testing of a feature $x$, each of the $M \times (M - 1)/2$ classifier votes for one class. The winning class is the one with the largest number of accumulated votes. In [24], it was shown that the one-against-one method is more practical for use then the other method, such as one-against-all.

For the SVM training, the input is a feature vector set of training images in which each image is manually annotated with a single category label selected out of $M$ categories. So, a set of $M$ labels are defined as $\{\omega_1, \omega_2, \ldots, \omega_M\}$, where each $\omega_i$ characterizes the representative global image category. In this context, given a feature vector $x$, the multiclass estimates the probability or confidence scores of each category as

$$p_m = P(y = \omega_m | x), \text{ for } 1 \leq m \leq M.$$  

The final category of a feature is determined based on the maximum probability score.

A. Classifier Combination

The feature descriptors as described in Section II are complementary in nature and represent image data that can lead to a better or robust classification result. There are two approaches to using different features: 1) concatenate features to a long composite vector and 2) use multiple classifiers on individual feature vectors—here the order and selection of classifiers of importance [25].

Four popular classifier combination techniques derived from Bayes’s theory, such as the product, sum, max, and mean rules [25] are considered for the expert combination strategies. Since the outputs of the classifiers are to be used in combination, the a posteriori probabilities in the range of $[0, 1]$ for each category will serve this purpose [15]. A multiclass SVM classifier on a combined feature space (e.g., early fusion) or several classifiers on individual feature spaces are combined or fused by the previous rules (e.g., late fusion) and finally classify the unknown query images to the category with the highest obtained probability value.

Algorithm 1 Classification-Based Image Filtering

For the SVM training, the input is a feature vector set of training images in which each image is manually annotated with a single category label selected out of $M$ categories. So, a set of $M$ labels are defined as $\{\omega_1, \omega_2, \ldots, \omega_M\}$, where each $\omega_i$ characterizes the representative global image category. In this context, given a feature vector $x$, the multiclass estimates the probability or confidence scores of each category as

$$p_m = P(y = \omega_m | x), \text{ for } 1 \leq m \leq M.$$  

The final category of a feature is determined based on the maximum probability score.

B. Image Filtering

We utilize the information about category prediction of query and database images for image filtering to reduce the search space. The output of the previous classification approach form a $M$-dimensional category vector of an image $I$, as follows:

$$p_j = [p_{j1}, \ldots, p_{jn}, \ldots, p_{jM}]^T.$$  

Here, $p_{jm}$, $1 \leq m \leq M$, denotes the probability or class confidence score that an image $I$ belongs to the category $\omega_m$ in terms of the feature vectors based on applying the previous early or late fusion strategies for classification.

During the offline indexing process, this outputs as category vector of the database images are stored as category index along with the feature indices in a logical database. When the system is searched based on an unknown query image, similar feature extraction and category prediction stages are performed online. The category vector of a query image $I_q$ based on (4) and the similar vectors of the database images (stored as a category index) are considered to find out whether a target image is a good candidate for similarity matching, thereby filtering out irrelevant images for further consideration.

In this approach, instead of only considering the image categories based on the highest obtained probability values, $n < M$ nearest classes of the query and target images are considered based on their sorted outputs of the classification. Next it is verified whether there is any overlap of classes between the query and target images. Generally, the value of $n$ is kept much smaller compared to the total number of classes $M$ in order to ignore the distant classes and perform the filtering effectively. A target image is only selected for further matching if at least one common category is found out between the top $n$ categories of the query image and itself. By performing this step, we decrease the risk of searching images entirely in a wrong place due to the classification error.

The steps of the filtering algorithm are presented in Algorithm 1.

IV. SIMILARITY FUSION

It is challenging to find a unique feature representation to compare images accurately for all types of queries. Feature descriptors at different levels of image representation are in diverse
forms and may be complementary in nature. In information retrieval (IR), more specifically in text retrieval, data fusion or multiple-evidence combination describes a range of techniques where multiple pieces of information are combined to achieve improvements in retrieval effectiveness [26], [27]. Many researchers have argued that better retrieval effectiveness may be gained by exploiting multiple query representations, retrieval algorithms, or feedback techniques and combining the results of a varied set of techniques or representations [27].

CBIR also adopts some of the ideas of the data fusion research in document retrieval. The most commonly used approach here is the linear combination of similarity matching of different features with predetermined weights. In this framework, the similarity between a query image \( I_q \) and target image \( I_j \) is described as

\[
\text{Sim}(I_q, I_j) = \sum_{F} \alpha^F S^F(I_q, I_j) \tag{5}
\]

where \( F \in \{\text{Concept}, \text{Keypoint}, \text{EHD}, \text{CLD}, \text{CEDD}, \text{FCTH}\} \) and \( S^F(I_q, I_j) \) are the similarity matching function (generally Euclidean) in individual feature spaces and \( \alpha^F \) are weights (generally decided by users or hard coded in the systems) within the different image representation schemes within our framework. However, there is a problem with the aforementioned hard-coded or fixed weight-based similarity matching approach. In this approach, for example, a color feature will have the same weight for the search of the microscopic pathology or X-ray images. Although, the importance of the color feature is negligible for many modalities, such as X-ray, CT, or MRI. The following sections present a fusion-based linear combination scheme based on the online category prediction of a query image.

### A. Category-Specific Similarity Fusion

In this approach, for a query image, its category at a global level is determined by employing the SVM learning. Based on the online category prediction of a query image, precomputed category-specific feature weights (e.g., \( \alpha^F \)) are utilized in the linear combination of the similarity matching function. Based on this scheme, for example, a color feature will have more weight for microscopic pathology or dermatology images, whereas edge and texture-related features will have more weights for the radiographs. The steps involved in this process are depicted in Algorithm 2.

From the previous algorithm, we can see that instead of using the predetermined hard-coded or fixed weight-based approach, the precomputed category-specific feature weights (e.g., \( \alpha^F \)) based on the online category prediction are utilized in the linear combination similarity matching function for each query.

### B. RF-Based Dynamic Similarity Fusion

A user might have a different interpretation of the semantic description in his/her mind or the prediction of the classifier might go wrong. Hence, it may be advantageous to have the option to interact with the system to refine the search process, such as RF. This section presents a RF-based similarity fusion technique where feature weights are updated at each iteration by considering both the precision and the rank order information of relevant images in the individual result lists based on the feedback from the users. As a result, the final rank-based retrieval is obtained through an adaptive and linear weighted combination of overall similarity fusing individual level similarities.

In this approach, to update the feature weights (e.g., \( \alpha^F \)), we at first perform similarity matching based on equal weighting of each feature. After the initial retrieval result, a user needs to provide a feedback about the relevant images from the top \( K \) returned images. For each ranked list based on individual similarity matching, we also consider the top \( K \) images and measure the effectiveness as

\[
E = \frac{\sum_{i=1}^{K} \text{Rank}(i)}{K/2} \times P(K) \tag{6}
\]

where \( \text{Rank}(i) = 0 \) if image in the rank position \( i \) is not relevant based on user’s feedback and \( \text{Rank}(i) = (K-i)/(K-1) \) for the relevant images. Hence, the function \( \text{Rank}(i) \) monotonically decreasing from 1 (if the image at rank position 1 is relevant) down to zero (e.g., for a relevant image at rank position \( K \)). On the other hand, \( P(K) = R_K / K \) is the precision at top \( K \), where \( R_k \) be the number of relevant images in the top \( K \) retrieved result. Equation (6) is basically the product of two factors, rank order and precision. The rank order factor takes into account the position in the retrieval set of the relevant images, whereas the precision is a measure of the retrieval accuracy, regardless of the position. Generally, the rank order factor is heavily biased for the position in the ranked list over the total number of relevant images and the precision value totally ignores the rank order of the images. To balance both the criteria, we use a performance measure that is the product of the rank order factor and precision. If there is more overlap between the relevant images of a particular retrieval set and the one from which a user provides the feedback, the performance score will be higher. Both terms on the right side of (6) will be 1, if all the top \( K \) returned images are considered as relevant. The raw performance scores obtained by the previous procedure are then normalized by the total score as \( \hat{E}(f^F) = \hat{\alpha}^F = E(f^F) / \sum_f E(f^F) \) to yield numbers in \([0, 1]\) where \( \sum_f \hat{E}(f^F) = 1 \). For the next iteration of retrieval, these normalized scores are utilized as the weights for the respective features in the linear combination of similarity
measures as
\[
\text{Sim}(I_q, I_j) = \sum_{F} \hat{\alpha}^F S^F (I_q, I_j) = \sum_{F} \hat{\alpha}^F S^F (\hat{f}_q^F, \hat{f}_j^F) \tag{7}
\]
where \(\sum_{F} \hat{\alpha}^F = 1\). The steps involved in the weight updating and similarity matching processes are described in Algorithm 3.

V. EXPERIMENTS

To evaluate the effectiveness of the proposed retrieval approach, exhaustive experiments were performed in a medical image collection. The collection comprises of 5 000 biomedical images of 30 manually assigned disjoint global categories, which is a subset of a larger collection of six different datasets used for retrieval evaluation campaign in ImageCLEF \(^1\) under the medical image retrieval track in 2007 [28]. In this collection, images are classified into three hierarchical levels. In the first level, images are categorized according to the imaging modalities (e.g., X-ray, CT, MRI, etc.). Next level is the image body-part, and the final level is the orientation. The categories are selected based on analyzing the visual and some mixed-mode query topics during the last three years (2005, 2006, and 2007) of ImageCLEF campaign under the medical retrieval task. Around 80\% of the images are gray level (e.g., X-ray, CT, MRI) and 20\% are color images (e.g., microscopic pathology, histology, dermatology) with varying resolutions.

A. Training

A training set of about 2 400 images is used for SVM learning to categorize images at a global level. The images are classified into one of eight modalities (viz., computerized tomography (CT), graphics (GX), magnetic resonance imaging (MR), X-ray (XR), positron emission tomography (PET), optical imaging (PX), and ultrasound (US)) as defined in the the modality detection task in ImageCLEF 2010 [29]. There can be considerable intraclass heterogeneity in this classification, e.g., the PX class contains both microscopic images as well as photographs. For the SVM training, the RBF kernel is used with a tenfold CV to find the best values of tunable parameters \(C\) and \(\gamma\). The kernel parameter \(\gamma\) controls the shape of the kernel and regularization parameter \(C\) controls the tradeoffs between margin maximization and error minimization.

The best values of \(C\) and \(\gamma\) for different feature representations are computed and used to train the SVM and generate model files. We use the LIBSVM software package [30] for the implementation of the SVM classifiers. For the local concept model generation based on the SVM learning, 30 local concept categories are manually defined, e.g., CT-Tissue-Brain, X-ray-Chest-Bone, etc. The training set consists of only 5\% images of the entire dataset of 5 000 images (i.e., 250 images). To generate the local patches, each image in the training set is at first partitioned into an \(8 \times 8\) grid generating 64 nonoverlapping regions. Only the regions that conform to at least 80\% of a particular concept category are selected and labeled with the corresponding category label. For the SVM training, we again use the RBF kernel with a tenfold CV to find the best values of tunable parameters \(C\) and \(\gamma\). After finding the best values of the parameters \(C = 200\) and \(\gamma = 0.02\) of the RBF kernel with a CV accuracy of 81.01\%, they are utilized for the final training to generate the local concepts model. We utilized the LIBSVM software package [30] for implementing the multiclass SVM classifiers for both global and local concept classification.

To construct the codebook of keypoints based on the Self-Organizing Map (SOM)-based clustering, the similar training set of images as used for local concept learning are utilized. To find the optimal codebook that can provide the best retrieval accuracy in this particular image collection, the SOM is trained at first to generate 2-D codebook of four different sizes as 256 \((16 \times 16)\), 400 \((20 \times 20)\), 625 \((25 \times 25)\), and 1600 \((40 \times 40)\) units. After the codebook construction process, all the images in the collection are encoded and represented as “bag of keypoints” as described in Section II. For training of the SOM, we set the initial learning rate as \(\alpha = 0.07\) due to its better performance. By comparing the retrieval performances based on precision recall, we finally choose a codebook of size 400 for the generation of the keypoints-based feature representation and the consequent classification and retrieval evaluation.

VI. RESULTS

To measure classification performance, we use a test set of 2620 images provided by the ImageCLEFmed\(^{10}\) organizers [29]. Individual classification accuracy is as follows: Concept: 71\%, Keypoint: 63\%, EHD, and CLD: 52\%, respectively, FCTH: 63\%, CEDD: 69\%, and Combined: 79%. The best accuracy is achieved when classification is performed in the combined feature space, but at the computational expense of a much larger feature vector. Different combination method accuracies are as follows: 80\%, sum: 80\%, max: 76\%, and mean: 79\%., which is in line with the observation in [25]. As expected, combining classifiers on uncorrelated and complementary features benefits the performance.

For a quantitative evaluation of the retrieval results, we selected all the images in the collection as query images and used query-by-example as the search method. A retrieved image is considered a match if it belongs to the same category as the query image out of the 32 disjoint categories at the global level. Precision (percentage of retrieved images that are also relevant) and recall (percentage of relevant images that are retrieved) are used as the basic evaluation measure of retrieval performances [18]. The average precision and recall are calculated

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\(^1\)http://www.imageclef.org/
over all the queries to generate the precision–recall (PR) curves in various settings. Fig. 2 presents the PR curves of the individual feature spaces when the similarity matching is performed based on applying the Euclidean distance measure. The performances are compared to a similarity fusion approach by providing equal weight to each feature in a linear combination. By analyzing Fig. 2, we can observe that the best performance is obtained in terms of precision at each recall level when the similarity scores are combined for individual features. More specifically, it is noticeable that the performance is improved in terms of early recall (e.g., 0.0–0.4) when compared to the best performed single concept-based feature. The performance of the proposed similarity fusion approaches is shown in Fig. 3. For the category-specific fusion, the weights of individual features are assigned as follows: 1) for medical imaging modalities (CT, MR, US, XR, NM, PET, and US), Concept, CLD, and EHD features are weighted equally (in general) and twice as much as the remaining features and 2) for photographs (PX), keypoint features are most significant. For RF-based fusion, we consider top 20 (e.g., $K = 20$) retrieved images from the previous retrieval iteration as the positive or relevant images to be considered for the fusion algorithm in next iteration. In the IR, community retrieval precision at the top 5, 10, and 20 retrieved items has been accepted as an adequate measure of performance. It is clear from Fig. 3 that the performance of the category-specific similarity fusion [e.g., Fusion (Category)] is improved when it is compared with the fusion based on equal weighting [e.g., Fusion (Equal Weight)] approach. In addition, the precision is further improved when similarity fusion is performed by considering one [e.g., Fusion (RF-1)] and two [e.g., Fusion (RF-2)] iterations of feedback information on top of the retrieval result obtained from the category specific fusion. In general, we achieved around 10%–15% performance improvement in precision at most recall levels (0.1–0.9) when our proposed similarity fusion approaches are compared to the equal weight-based similarity fusion. Overall, from the PR curves in Fig. 3, we can conjecture that the supervised learning, either in the form of classification or RF, helps to improve the retrieval results in terms of precision.

To test the retrieval effectiveness of the RF-based similarity fusion in terms of the number of top retrieved images as relevant one, experiment is performed with $K = \{10, 20, 30, 40, 50\}$ as shown in Fig. 4. The performances are compared by considering only one iteration of feedback information. From Fig. 4, it is observed that the best performance is achieved when we consider only top ten images (e.g., $K = 10$). There is a decrease in performances when the number of $K$ increases as shown by the PR curves in Fig. 4. One possible reason is that due to the automatic feedback for experimental purpose, there can be many irrelevant images being considered as relevant when the number of $K$ increases and this affects the retrieval performance. On the other hand, this is actually a benefit for an interactive system like this as the users need to judge less images to provide feedback information to achieve an optimal precision.

To check the consistency in RF-based similarity fusion in terms of the number of iterations, we also consider 5 iterations of feedback and compared the performances by calculating average precision within the top 20 [e.g., $P(20)$] retrieved images. The performances are compared by considering only one iteration of feedback and two different setting for $K = 10$ and $K = 20$. As the system converged, it was observed that the retrieval performance is consistent across number of iterations and for different values of $K$.

Finally, the retrieval experiment was performed with and without filtering on different fusion-based approaches to test the effectiveness and efficiency of the proposed method. Top three ranked category labels were used for the experiment and applying the similarity fusion approaches in the filtered image set, we achieved same PR curves as depicted in Fig. 3. This suggests that search performed on a relevant subset of image collection does not cause any degradation in retrieval accuracy due to the fact that the filtering algorithm only discard those images. Further, an important benefit of searching on a filtered...
image set is gain in computation time. We tested the efficiency of the fusion-based search schemes by comparing the average retrieval time with and without applying the filtering scheme. The experiment was performed in an Intel Pentium Dual-Core CPU at 3.40 GHz with 3.5 GB of RAM running Microsoft Windows XP SP2 Professional operating system. The linear search time without filtering was twice as much as search on the filtered image set, suggesting that the proposed method is both effective and efficient.

VII. CONCLUSION

In this paper, a novel learning-based and classification-driven image retrieval framework is proposed for diverse medical image collections of different modalities. In our approach, we directly link classification to retrieval. In this framework, the image category information is utilized directly to filter out irrelevant images and adjust the feature weights in a linear combination of similarity matching. We use the RF-based technique to update the feature weights based on positive user feedback. Retrieval performance is promising and clearly shows the advantage of searching images based on similarity fusion and filtering in terms of effectiveness and efficiency. Overall, this retrieval framework is useful as a front end for large medical databases where a search can be performed in diverse images for teaching, training and research purposes.

ACKNOWLEDGMENT

The authors would like to thank the CLEF [28], [29] organizers and the Radiological Society of North America (RSNA), for making the database available.

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Authors’ photographs and biographies not available at the time of publication.